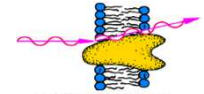


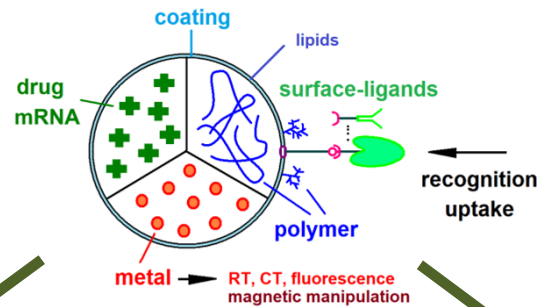
Nano-structure Development of Oral Pharmaceutical Formulations in Simulated Intestine – D-contrast SANS and DLS



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- 1) Gutenberg-University, IPBW Institute Pharmacy Biol. Life Sci., Pharm.-Technology, D-55099 Mainz, Germany
- 2) Kwame Nkrumah University of Science and Technology KNUST, Department of Pharmaceutics, Kumasi, Ghana
- 3) ILL, Institut Laue Langevin: LSS / D11, BP156, Avenue des Martyrs, F-38042 Grenoble, France
- 4) JCNS - MLZ, Jülich Centre for Neutron Science, FRM-II Reactor, D-85748 Garching, Germany

Therapeutic Nanoparticles as Drug carriers: Mixed nanoparticles bearing material domains



Combination : **DLS** and **SAXS** and **D-contrast Neutron scattering SANS**

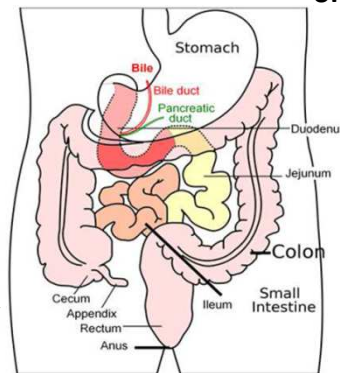
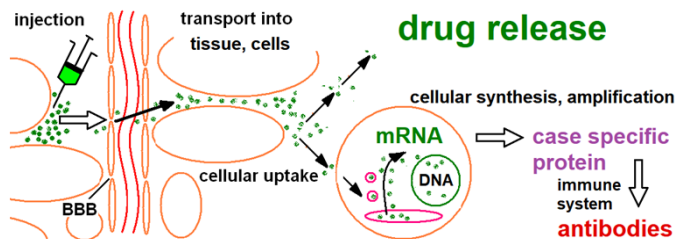
Therapy material development

< Poster 238 >

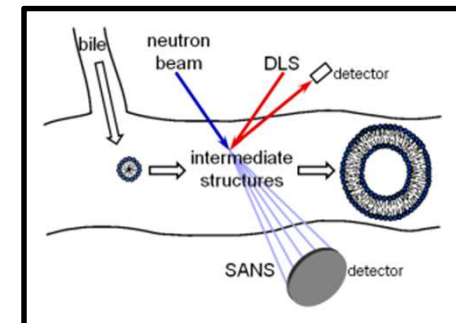
< Poster 241 >

(I)
Parenteral (injection) :
study of formulations and interactions

(II)
oral (tablet, capsule, solution) :
study in a Gastro-Intestinal simulator models (GI-Sim)



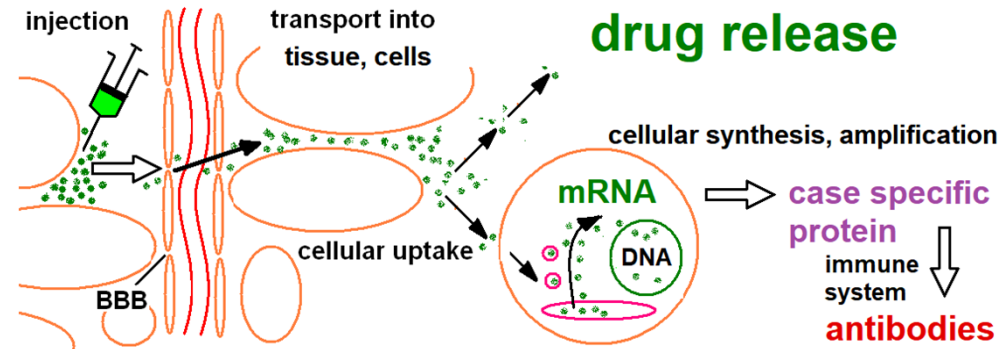
study in a Gastro-Intestinal simulator models (GI-Sim)



Therapy method development
Immuno-therapy (mRNA)
Vaccination

(III)
tissue- and cell bio-targeting
< Poster 238 & 241 method page >

(I) Parenteral drugs in nanoparticles



Drug nanoparticles for parenteral application (injection): The drug (pharma agent, mRNA) in lipid, liposomes or polymer nanoparticles release the drug, **if the structure is sufficient**.

- A) Conventional parenteral drugs:** release the drug (pharma agent) from solution or nanoparticles **non-specific**.
- B) mRNA nano-drugs :** code for the cellular synthesis of a specific protein, which later induces antibody generation. This implies a double **amplification** (> 1000 x) by cell elements (ribosomes, T-Cells)

mRNA is :

- **not toxic**, as it is a native cellular intermediate (short-life work-copy of a gene)
- **sensitive**, as cells and tissue switch it off quickly by enzymatic **degradation** (RNase) temperature and hydrolysis sensitive , need sterility and cooling, if **pure**
- **Nanoparticle structure** embedding can stabilize, and facilitate cell uptake (activity)

Analogy in a computer – CNC system:

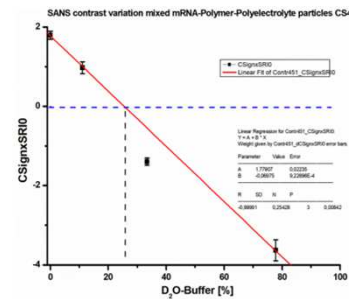
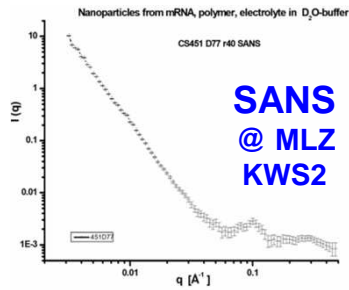
1 Harddisk (DNA) \Rightarrow 20 file-copies on USB-Sticks (mRNA) \Rightarrow 1000 products by 3D-printer set (ribosomes)

mRNA-Nanoparticles for immuno-therapy : two forms

(1) mRNA polymer nanoparticles

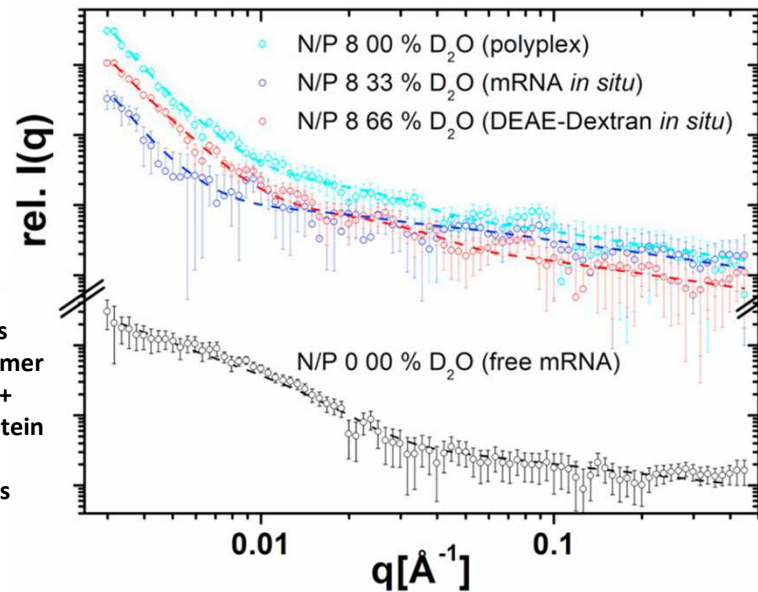
SANS with Deuterium-contrast variation \Rightarrow component domains in drug nanoparticles

mRNA in AminoDextrane NP's

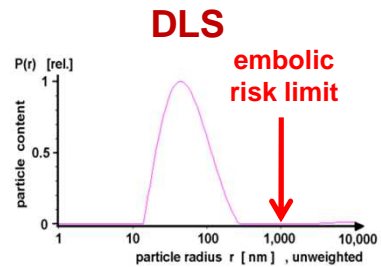
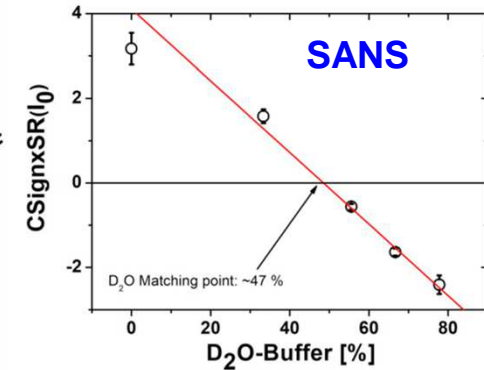


Improvements
a) charged polymer
b) basic lipid+ polymer, protein
Core-shell-NP's

mRNA in DEAE-Dextrane NP's



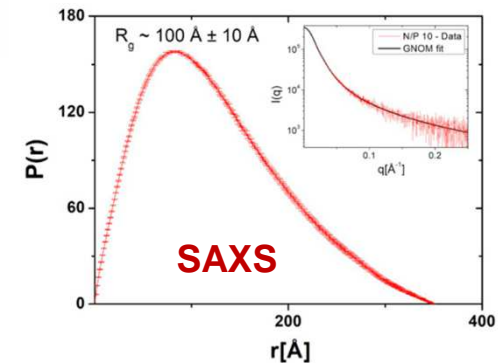
Siewert C, Haas H, Nawroth T, Sahin U, Langguth P et al. (2019) **Biomaterials** 192, 612-20: mRNA-DEAE-Dextran polyplexes SANS & DLS



DLS as med. security test

mRNA immuno Nanoparticles:
Medical use for :
a) vaccination, e.g. Covid-19
b) cancer immuno therapy
Structure based development :
variant coding for luciferase
SANS, SAXS, DLS, animal tests

mRNA nanoparticles for immuno-therapy :
MLZ FRM-II, KWS2
DESY-Petra III , P12

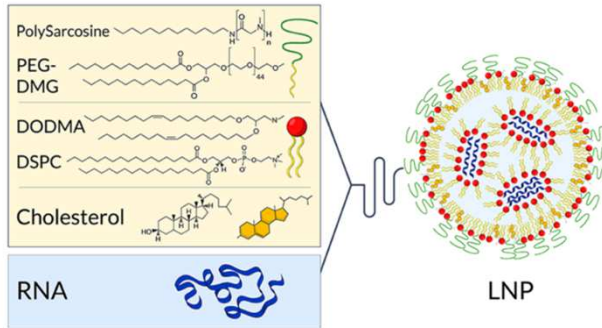


Siewert CD, Haas H, Cornet V, Nogueira S, Nawroth T, Uebbing L, Ziller, A, Al-Gousous J, Radulescu A, Schroer MA, Blanchet CE, Svergun DI, Radsak MP, Sahin U, Langguth P (2020) **Cells** Doi 10.3390/cells9092034 mRNA-Lipid-Polymer complexes SANS, SAXS, DLS

with
M. Schroer,
D. Svergun
C. Blanchet

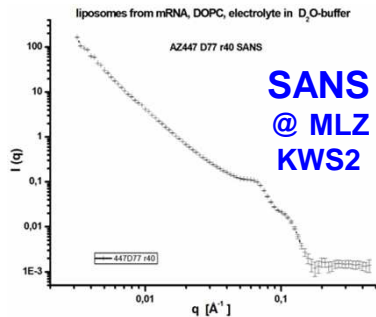
mRNA-Nanoparticles for immuno-therapy : two forms

(2) mRNA lipid-layer nanoparticles



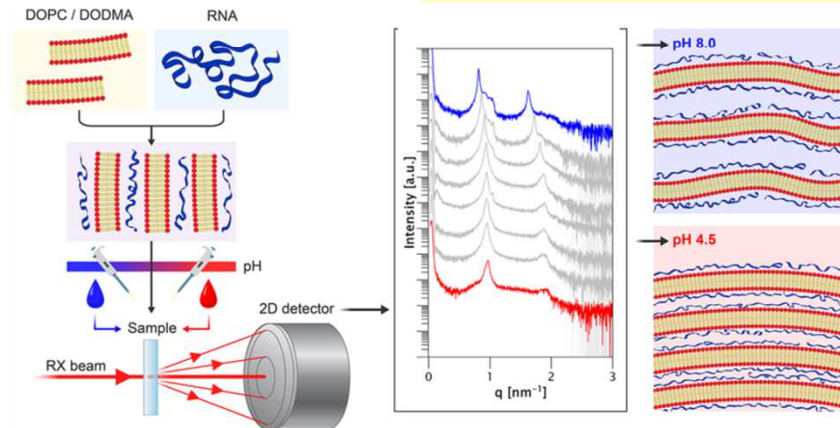
mRNA is assembled with lipids: charged, neutral and extended hydrophilic headgroups. Sequential mixing, shearing in a pH-regime results in spherical solid lipid nucleo particles (LNP), or multilayer nanoparticles (below), depending on the charge-lipid-head ratio.

Uebbing L, Schroer MA, Svergun D, Sahin U, Haas H, Langguth P et al. (2020) *Langmuir* 10.1021/acs.langmuir.0c02446
pH-response of mRNA NP's



SANS
@ MLZ
KWS2

SANS of mRNA in non-charged liposomes (DOPC)

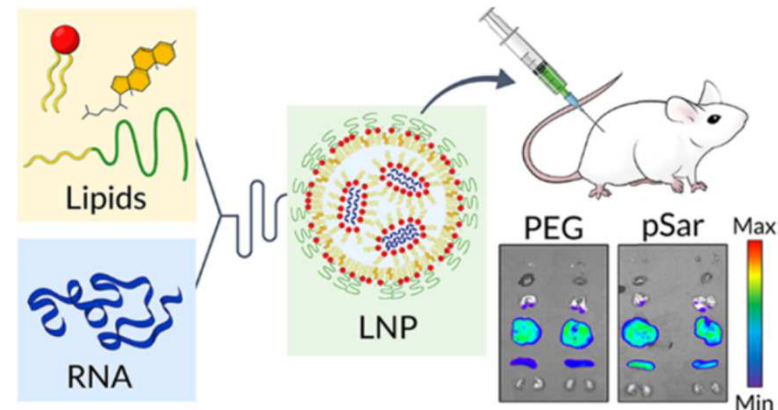


DESY-Petra III , P12

Nogueira SS, Svergun D, Langguth P, Sahin U, Haas H et al. (2020) *Applied Nano Materials* doi 10.1021/acsnm.0c1834
Polysarcosine-mRNA NP's, SAXS, DLS, animal tests

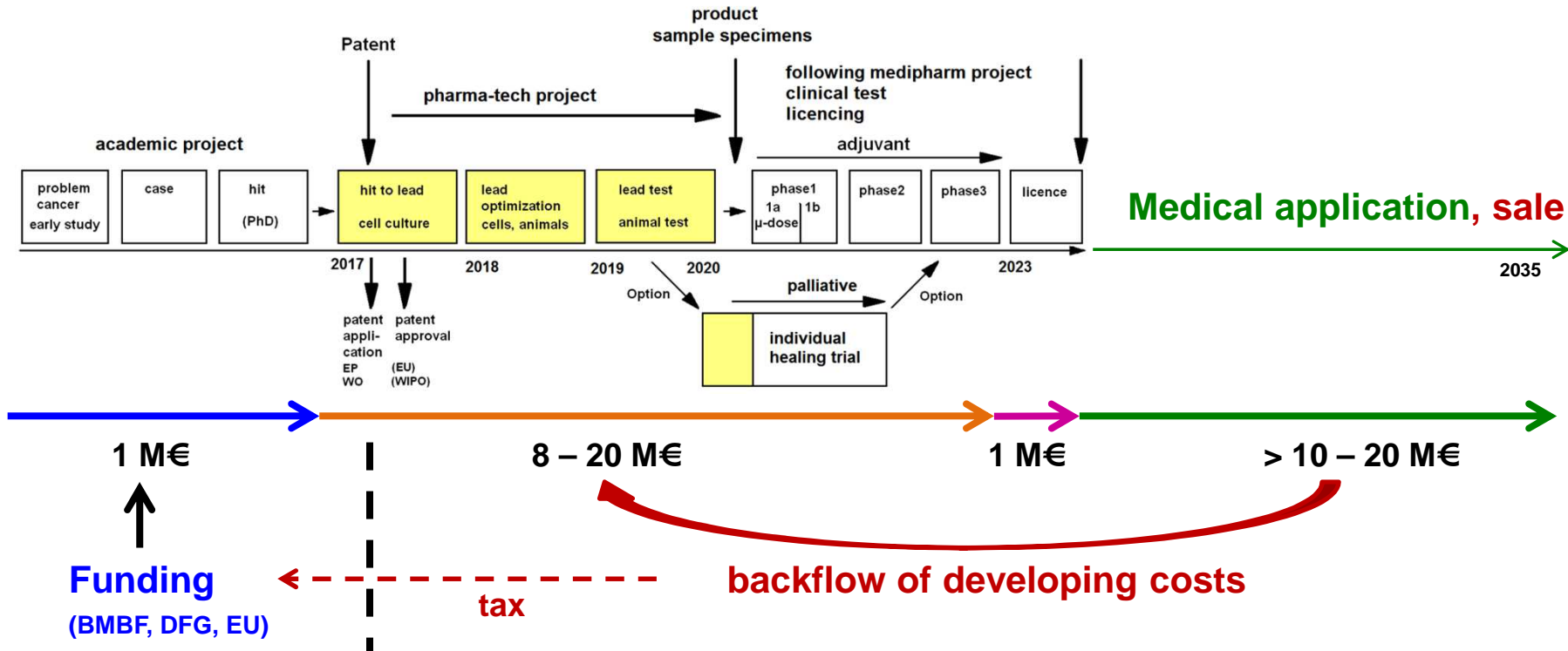
further
SANS
beamtime is
applied

For **structure based nanoparticle development** a mRNA variant is chosen, which codes for luciferase (the light generator of fire fly). Thus the medical success of a mRNA nanodrug treatment (cell uptake and induced protein synthesis) can be proven in an animal test (mice) by light generation: the active regions get luminescent.



Nanoparticle & Therapy – Licencing and Patents

no medical use without patent and licence possible



Pharma-product development and licencing steps: 8 -10 years , costs ~ 20 mio €

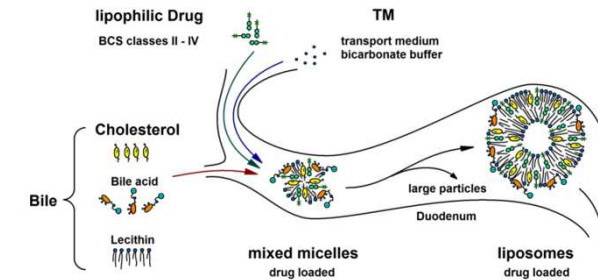
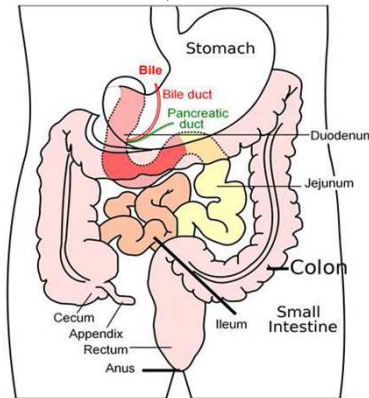
- Fast licencing, emergency licence ~ individual healing trial ; e.g. in case of Covid-19
- Development and licencing can be accelerated by fast bioequivalent lab methods, e.g. a **drug application simulator device** ⇒⇒ second part of the presentation

Pharma-Nanoparticles II : Drug application simulation

Transient nanoparticles from oral forms in the human digestion system (GI)

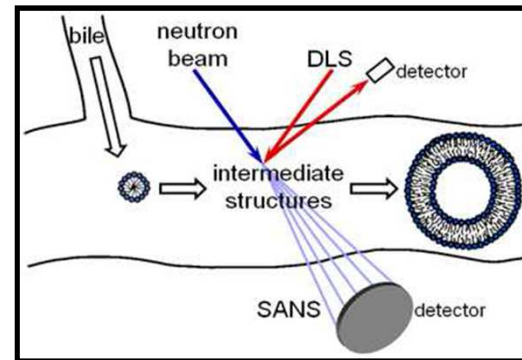
FaSSIF-C : GI-model fluid with cholesterol nanoparticles

Drug (tablets, capsules) :
stomach



Gastro-Intestinal –Simulator device (GI – Sim)

20 min.



Particle size scale: 5 nm – 200 µm !

⇒ **TR-SANS + DLS**

The micelle to liposome **structure development** in simulated intestinal fluid (FaSSIF) was detected by **time resolved SANS + DLS**. (ILL-D11, and @ FRM-II KWS2)

Nawroth T, Buch P, Buch K, Langguth P, Schweins R (2011) Mol Pharmaceutics 8, 2162-72

At **FRM-II KWS2** a set of cholesterol based **bioequivalent model fluids “FaSSIF-C”** for the *in vitro* study of intestinal drug resolution and uptake in the duodenum was developed. The drug solubilization capacity was related to the nanostructure estimated by DLS and neutron scattering SANS; bio-equivalent location: **2nd half of duodenum**

Khoshakhlagh P, Johnson R, Langguth P, Nawroth T, Szekely N.K., et al. (2015) J Pharm Sci 104, 2213-24
.. FaSSIF-C **with Cholesterol** ⇒ **Study with 8 drugs** (2015-2020: R. Johnson, P. Thumarati, V. Stahl)

- Interaction of BCS2/4-
drugs in nanoparticles,
with intestinal model fluids
and transient nanoparticles
therein (intermediates)

- 8 Drugs:

- **BCS2:** Fenofibrate, Danazol, Griseofulvin, Carbamazepin, Paracetamol, Gemcitabin, Curcumin; in **nanoparticles**
- **BCS4:** Amphotericin B, Amphotericin B - Cholesterol (SL Dr. R. Johnson, Ghana)

- Methods combined (time resolved):

- Drug solubility (in FaSSIF, FaSSIF-C)
- DLS (time resolved): micelles, liposomes, large NP's
- SANS (time resolved) at FRM-II, Muni-Garching

- Intestinal model fluids,
physiological relevant:

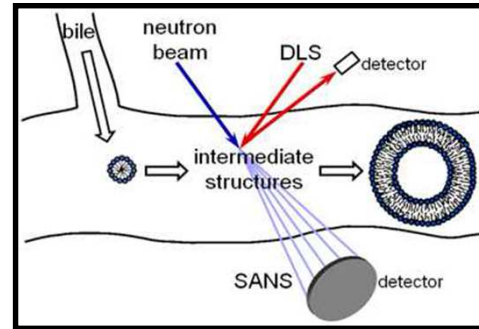
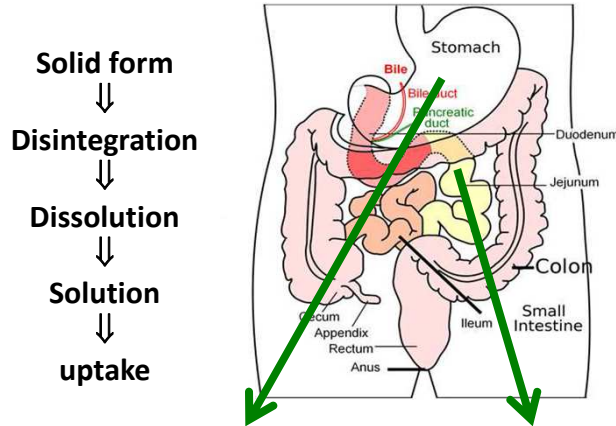
- FaSSIF_{mod6.5}: pH-stabilized (BiCarbonate+HEPES)
- FaSSIF-C, pH-stabilized, containing Cholesterol (as bile)



Solid form \Rightarrow Fragments mm \Rightarrow Microparticles μm \Rightarrow Nanoparticle development : Liposomes \Rightarrow Micelles \Rightarrow Solution

Drug (tablets, capsules)

Particle size scale: 5 nm – 200 μm !



Gastro-Intestinal –Simulator device (GI – Sim)

\Rightarrow **TR-SANS + DLS**

Oral drug formulation development for difficult drugs : BCS 2, 4 , (3)

Duties of a GI-Simulator :

- Interaction of **BCS2/4-drugs** in nanoparticles, with intestinal model fluids and **transient nanoparticles** therein (intermediates)
- **Licensing process** of drug formulations : kinetics
- **Food effect**, viscosity
- **Comparison** of pharmaceutical products, generic products
- **Methods** combined in GI-Sim:
 - **Drug solubility and uptake** (time resolved, in FaSSIF-C)
 - **DLS** (time resolved): **size and kinetics** of micelles, liposomes, large NP's
 - **SANS** (time resolved) **structure and dynamics** of nanoparticles

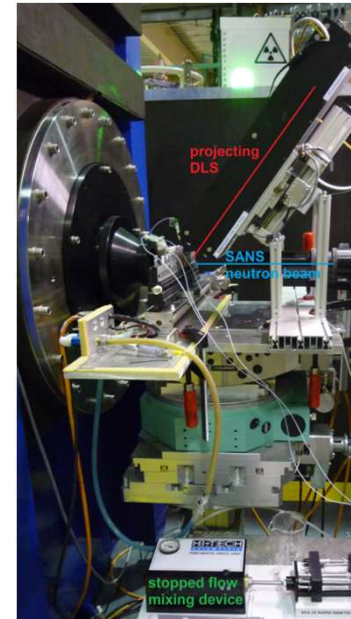
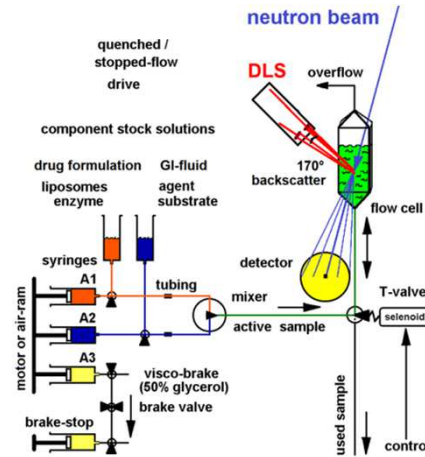
GI model	stomach	intestine	Technology, particle	drug form development
GiSim 1	mixing, pH-jump, stirring	vessel, cuvette, static („pot“)	Stopped flow, fast mixing, 100 nm NP	Solid to disintegration and dissolution, nanoparticles, time
GISim 2	mixing, pH-jump, stirring	flow through, closed channel	Continuous flow, syringe pumps, 100 nm	Solid to dissolution to nanoparticles, localized
GISim 3	stiring, pH-shift, pressure, flow	flow through, series of vessels	GI-Batch flow (n x 50 ml), peristaltic pumps for micro-particles (50 μm)	Stepwise tablet (solid) nano-disintegration and dissolution to nanoparticles
GISim 4	stiring, pH-shift, pressure, flow	flow through, series of vessels	GI-Batch flow, spiral pumps for large particles (2 mm)	Stepwise coated tablet disintegration to μm particles, later intestine dissolution to NP
GISim 5	stiring, pH-shift, pressure, flow	flow through, open channel, then vessels	GI-Batch flow, spiral pumps, solid form / tablet transport (2 cm)	Enteric coated tablet (solid) disintegration in intestine, dissolution to nanoparticles

Gastro-Intestinal simulator designs for the *in vitro* study of stepwise drug form disintegration, dissolution (resolution): The technology is related to the micro- and nanostructure estimated by **projecting DLS** (10 nm – 200 μm) and neutron scattering **SANS** (1-200 nm), **SAXS** option.

Gastro-Intestinal – Simulator devices (GI – Sim)

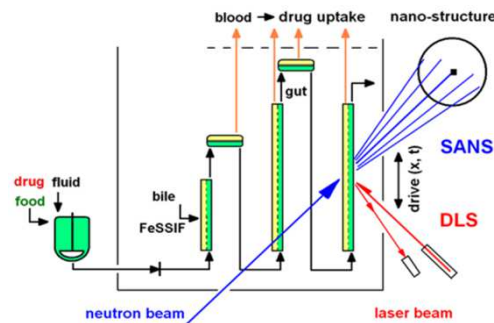


GI Sim 1 :
one shot mix



GI Sim 1 setup for
SANS+DLS with a
stopped-flow mixer
at ILL D11

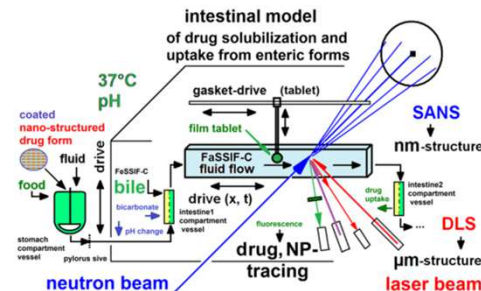
- GI Sim 2: flow-through
- GI Sim 3, 4: batch flow (n x 50ml) multi-vessel
- GI Sim 5: coated solid form transport



The frame with the flow-channel (Quarz, 200x12x2 mm) is moved in the beam



GI Sim 2 setup for
SANS+DLS with
flow-through pumps
at MLZ/JCNS KWS2



DLS as q-range
 extension for
 large drug-
 particles

 SANS for
 nanoparticles



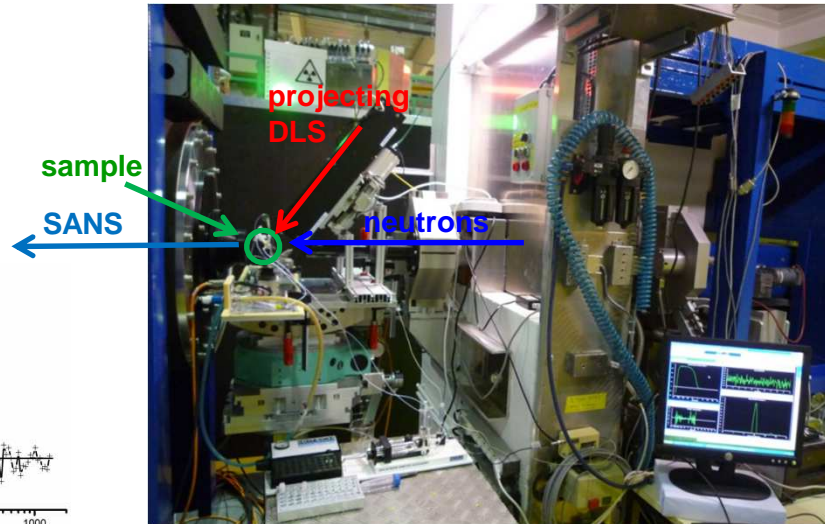
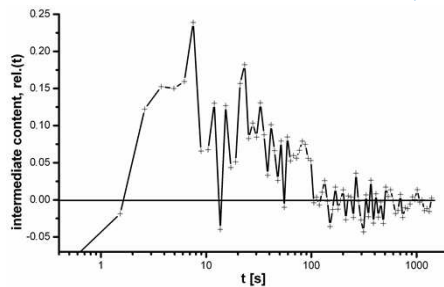
Stopped-flow Simulator **GISim1** with combined **SANS+DLS** Nanoparticle development in Intestinal model fluid

D11

ILL-D11 :

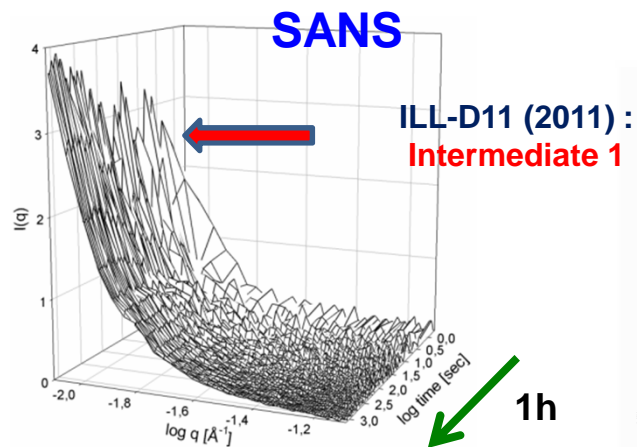
SANS:

Intermediate 1
in intestinal fluid

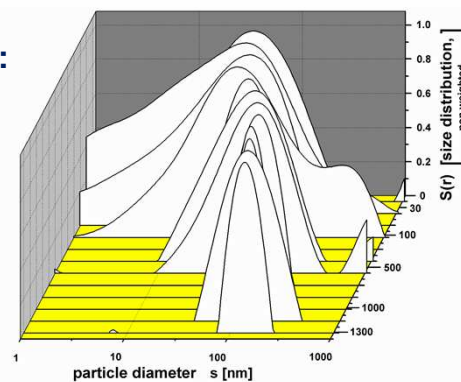


ILL-D11 : setup

time resolved :



+ DLS:



- FaSSIF_{mod6.5}: pH-stabilized **intestinal model fluid**
 - HEPES as pH stabilizer
 - physiological osmolality
- Nanostructures develop in time after dilution (FaSSIF to FaSSIF, **bile influx in gut**)
 - time resolved **DLS (@university-lab and with SANS)**: large structures <50µm, but limited precision
 - time resolved neutron scattering **SANS**: high precision, component resolution by **partial deuteration, 71% D₂O**

• SANS-Facilities :

1. ILL, Grenoble (D11)
2. FRM2, Munich-Garching (KWS2)

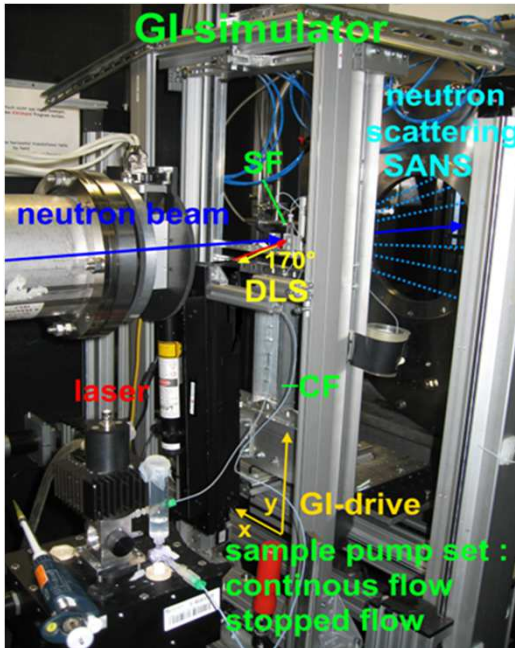
• Results:

- Intermediate nanostructures detected at ILL (Grenoble) and FRM-II (Munich-Garching)
- Components resolution by deuterium matching with D₂O-solvent possible (see <2> HST)
- Drug contribution: Fenofibrate, Danazol, Griseofulvin, Curcumin (FRM-II KWS2, GI-simulator)

Nanoparticle development : Micelles (bile) ⇒ Liposomes ⇒ Micelles ⇒ Solution

Cooperation: **Ralf Schweins**
ILL Grenoble, LSS group

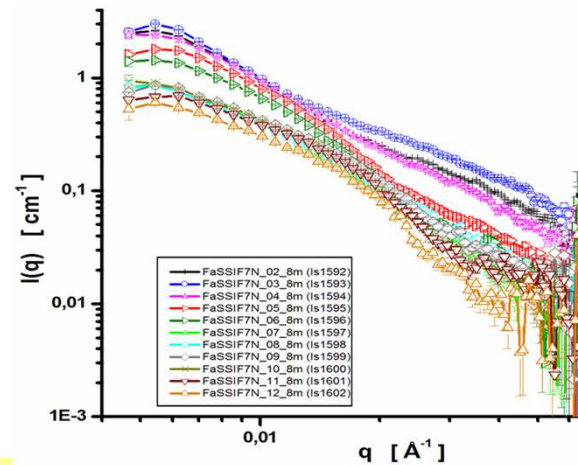
xtr-SANS + DLS
flow-trough pumps
⇒ steady-state
Quarz-channel
200x12x2 mm



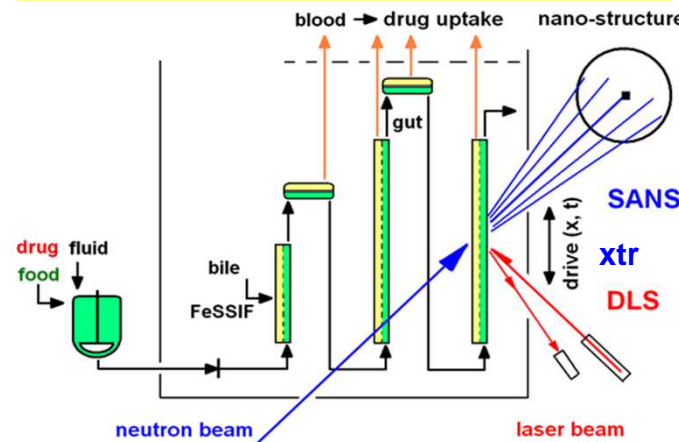
GISim 2 simulator,
drug uptake and digestion
simulator concept,
NP structure analysis:
continous flow CF

Drug analysis:

- gut & blood side (layers)
- membrane separator - gut
- drug nano-dissolution



Detection:
- drug-transfer (dialysis cells)
- **DLS** (x,t resolved)
- **SANS** (x,t resolved)



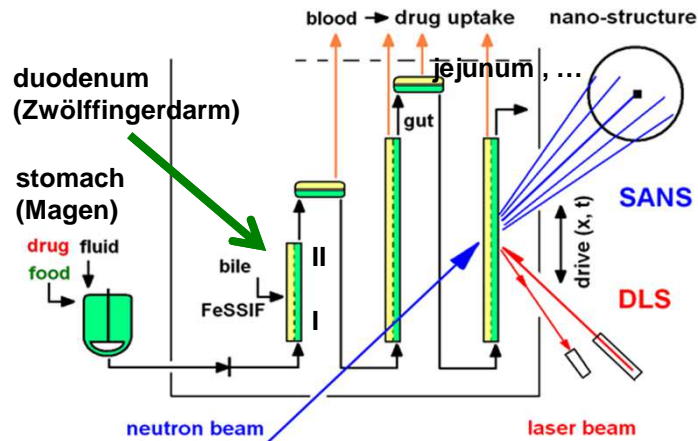
- **Parallel tracing** of :
- drug solubilization
- nanoparticle structure
- model uptake/ transport
- **Time- and local resolved drug & nanostructure profiles (2D)**
 $C_{drug}(x,t)$ for gut and blood side
- **SF: Stopped flow (duodenum-2)**
for fast events (<20 cm, <20 min
after bile influx into the Duodenum)
- **CF: Continous flow** (flow through)
model device for **full simulator**
- module concept (flexible)
- two compartment/ channels
- long modules: uptake-dialysis
- short modules: cell layer, gut
- **Drug x-t-profiles:** time-local
resolved sampling
- **Nanostructure estimation:**
- x-t profiles
- DLS as overview (+-20%), in lab
- neutron scattering SANS for precision
and deuterium contrast
- **Resolution** of nanocarrier and
drug:
- for neutrons by deuteration (lipid, solvent
contrast D_2O -matching)

- option for improved tracing:
FCPS (DLS with fluorescence)

T. Nawroth, K. Buch, P. Langguth, R. Schweins; (2011) *Molecular Pharmaceutics* / 8, 2162-72
 Khoshakhlagh P., Johnson R., Nawroth T., Langguth P., Szekely N.K., et al. (2014) *Eur J Lipid Sci Techn.* 116, 1155-66
 Johnson R., Nawroth T., Khoshakhlagh P., Langguth P., Szekely N.K., et al. (2014) *Eur J Lipid Sci Techn.* 116, 1167-73
 Khoshakhlagh P., Johnson R., Langguth P., Nawroth T., Szekely N.K., et al. (2015) *J Pharm Sci* 104, 2213-24 .. FaSSiF-C

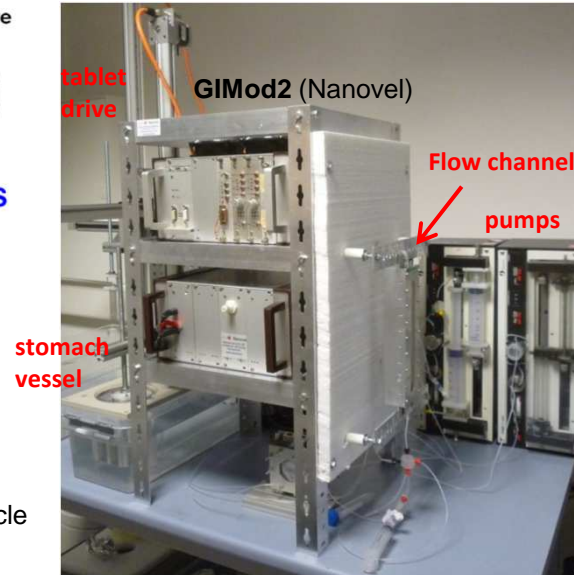
Continuous Flow (GSIM 2): time-space Resolution xtr long Quartz-cell with continuous sample-mix supply

V1 @ FRM-II_KWS2 : **SANS + DLS**



The continuous flow (CF) modules simulate the gut segments (total: 6m; ~12h). In the channel nanoparticle structure develops in time and space ($dx = dt$).

V2 @ Pharma-Lab : **DLS+sampling**



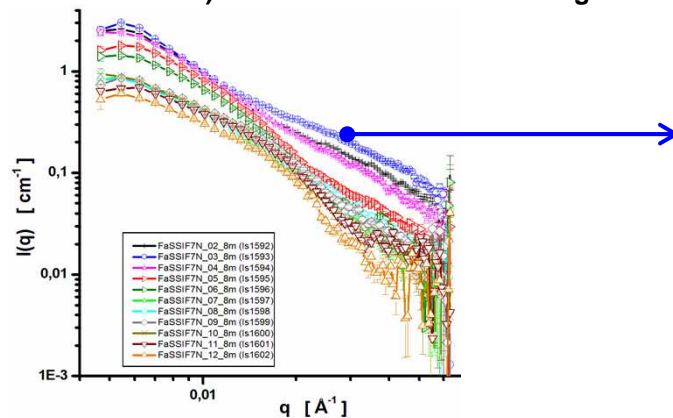
Continuous flow (CF) study of simulated intestinal colloids:

- Nano-development in **time & distance** : x, t
- Long Quartz flow-through channel (cuvette)
- Mixer in front (fluids + bile; by pumps)
- SANS + DLS investigation (online or offline)
- Large structure investigation *in situ* by **projecting DLS**: 50 nm – 200 μm (ProSpecD: Nanovel)

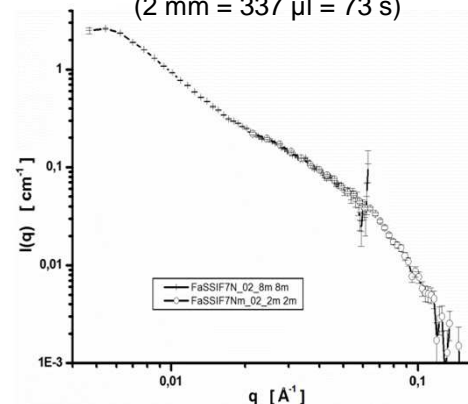
CF results at FRM-II_KWS2:

- Modules with melt-drawn Quartz ok.
- Duodenum-II : segment after **bile** influx, **71%D₂O**
- Shortest time (first frame @ 2mm) ~337 μl after mixing of model bile with fluid from stomach (TM)
- Inspection by: **a) DLS, and b) neutrons, SANS**, CF-module on a CNC-drive) : well statistics
- novel **bio-equivalent model intestinal medium** FaSSIF-7C, **containing 7% cholesterol**
- Excipients (detergents+ targeting lipids)
- Core-shell drug polymer nanoparticles and lipid particles

Duodenum-II: a) CF-distance evolution during 30min.



b) shortest frame – distance (2 mm = 337 μl = 73 s)



CF SANS at FRM-II_KWS2: The development of diluted bile in a long flow-through cuvette (160x18x2 mm) from micelles to liposomes and large particles, with cholesterol containing model fluid FaSSIF-C (7% cholesterol)

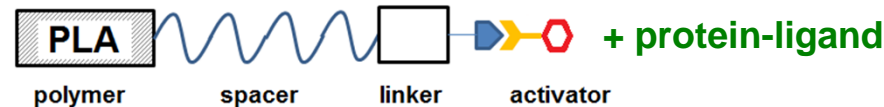
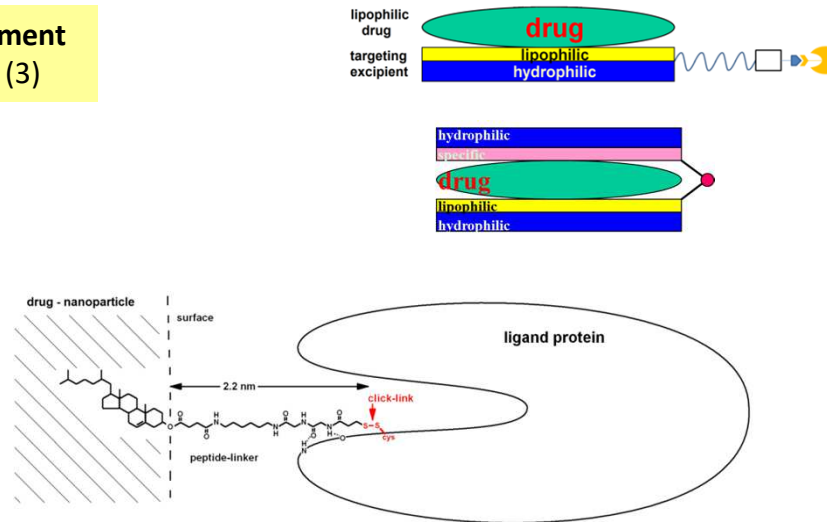
Cooperation:

Aurel Radulescu, Noemi Szekely
FRM-II, JCNS, KWS2

(III) Bio-Targeting and Bio-availability : targeting by ligands/ proteins at the particle surface

Oral drug formulation development
for difficult drugs : BCS 2, 4 , (3)

		solubility	
		+	-
drug uptake	+	BCS 1	BCS 2
	-	BCS 3	BCS 4



principle:
4 domain
targeting-exciptent

Cholesterol-
targeting construct

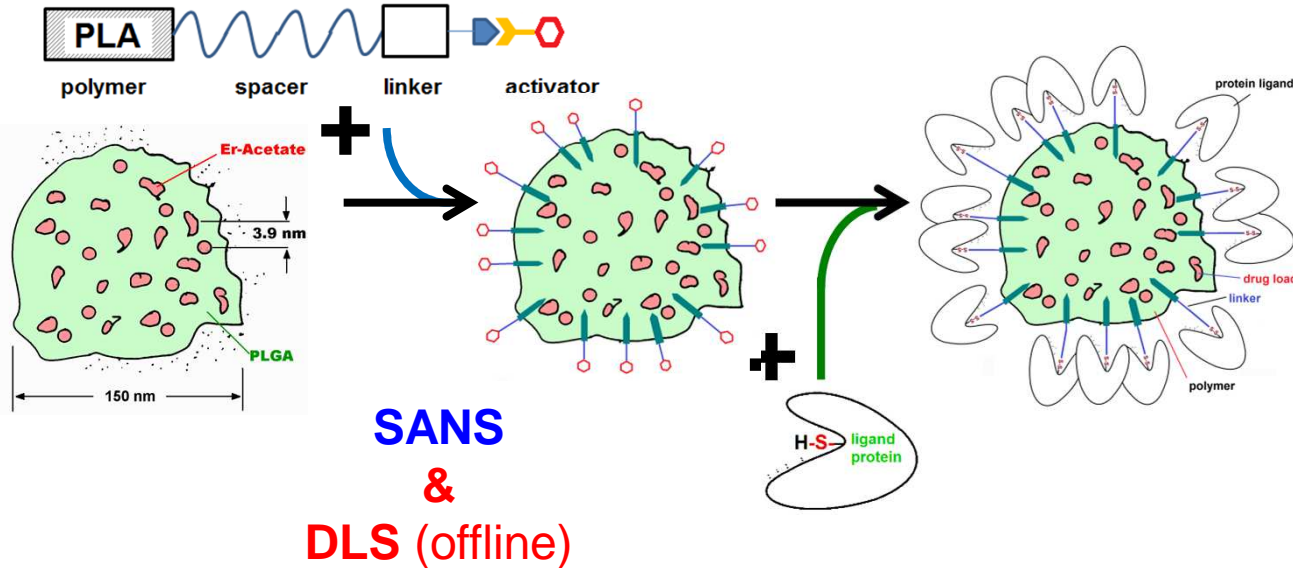
Polymer-
targeting construct

- **Cancer problem:** in 95% of the cases, the disease is individual different at cell level
- => **Concept of individual therapeutics by case selective surface modification**
 - transport of anti-cancer drug by nanoparticles (10,000,000 drug molecules / particle of 100 nm size); for radiotherapy: Lanthanides, Isotopes (Er, Gd, Lu, ¹⁰B, Pt, Bi); or/and chemo-therapeutics
 - Individual modification of pre-manufactured Nano-carriers (coated) as very last step (1 day, „click-link“)
 - The surface ligand(protein) is recognized by over-expressed receptors of the cancer cell => endocytosis
- **Drug carrier and linker development:**
 - Domain structure and linker conformation (ligand exposition) **SANS + DLS** : **Deuterium-contrast SANS**
- **Product Quality control** : **DLS + SANS** for **medical security** (embolic risk exclosure)

Target Polymer Nanoparticles as drug carriers

PLGA triple component NP for modification by Ligands (Proteins)

PLGA w/o/w nanoparticles (10% heavy metal) => cell target nanoparticles



Cooperations:
Ralf Schweins
ILL Grenoble, LSS group

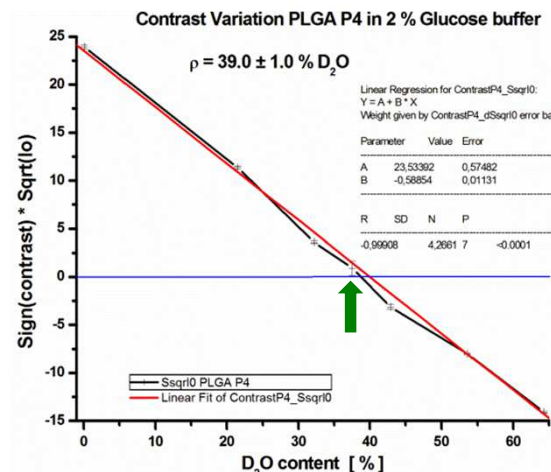
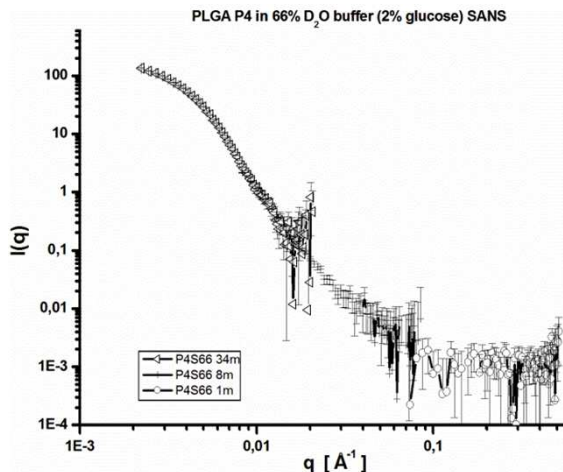
FRM-II, MEDAPP

PLGA w/o/w triple NP's
double emulsion + protein
prepared from activated
target-polymer: 2% PLA,
98% PLGA (Resomer 502H)

- **D-contrast variation SANS**
SANS + DLS

- **Ligand-protein** loading on **D-matched target-PLGA NP** upon time-resolved SANS of D-contrast matched polymer nanoparticles (PLGA w/o/w)
- **Cell targeting** nanoparticles with surface-protein ligand as final product: non-toxic, bio-degradable; for **RT & CT**

ILL-D11 (2015) : **SANS + DLS** of PLGA (w/o/w) NP with activated targeting polymer



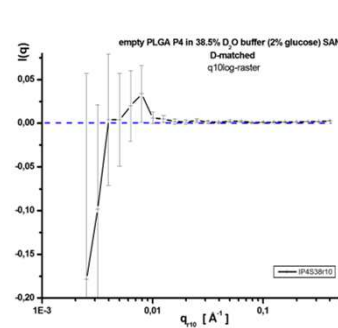
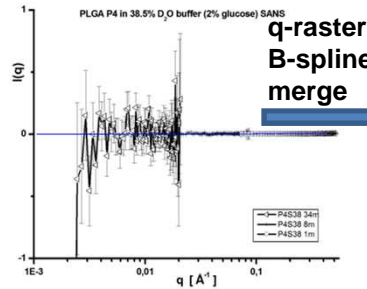
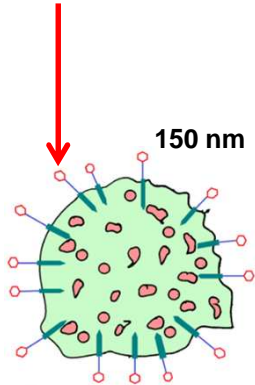
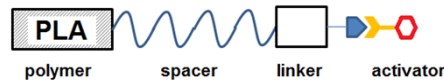
Target Nanoparticles Polymer for Cancer Therapy

PLGA triple component NP : modification by Ligands (Proteins)

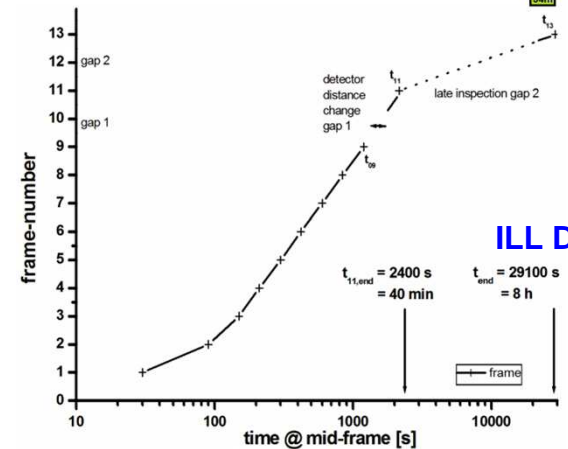
PLGA w/o/w nanoparticles loading by SH-protein => **cell targeting nanoparticles**

ILL-D11 : TR-SANS + DLS of PLGA (w/o/w) NP with activated targeting polymer + protein

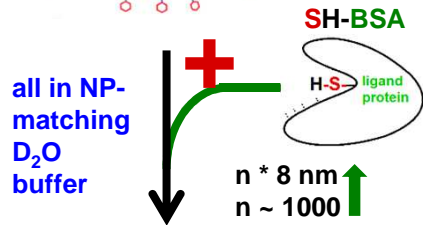
Cooperation: Ralf Schweins, ILL Grenoble, LSS group



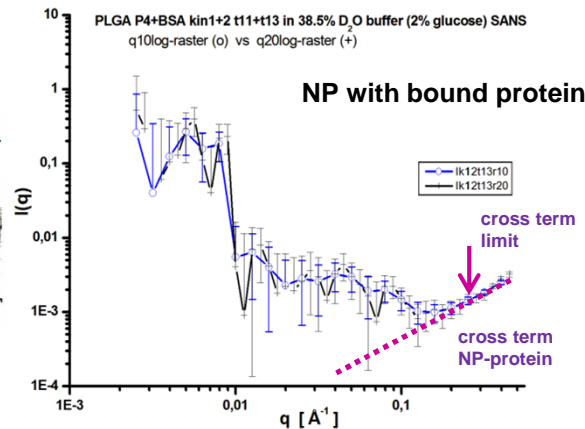
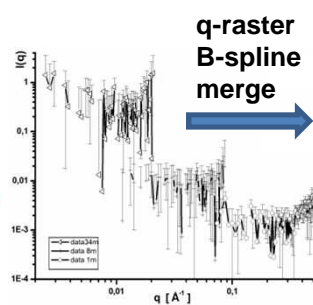
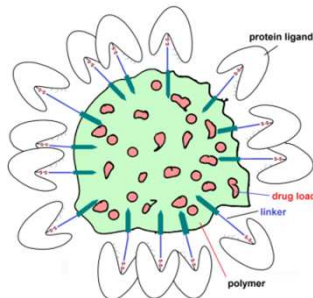
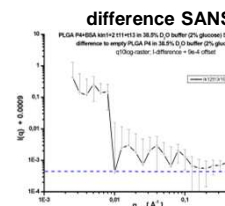
TR-SANS : twin shots of time resolved SANS and detector distances d



ILL D11



Protein coupling of
D-contrast matched
Polymer nanoparticles
for individual therapy



SANS of protein-loaded polymer nanoparticles (PLGA w/o/w) in polymer-matching D₂O buffer: logarithmic q-rastering for noise reduction

- **D-contrast variation SANS TR-SANS + DLS**
- **Ligand-protein loading on D-matched target-PLGA NP** upon time-resolved SANS of **D-contrast matched** polymer nanoparticles (PLGA w/o/w)
- noise reduction by q-rastering
- current work: improvements for stabilization by surface coatings

Target Nanoparticles : Stabilization by Coating mixed shell of Polymer, Lipids and Ligands (target-Proteins)

1) Hydrophobic drug nanoparticles coating by lipid+gelatin => stable nanoparticles



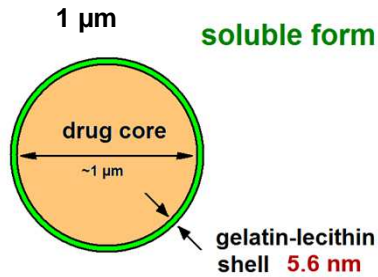
Cooperation: Aurel Radulescu, Noemi Szekely, FRM-II, JCNS, KWS2

hydrophobic drug

Amphotericin B

Lecithin

Gelatin

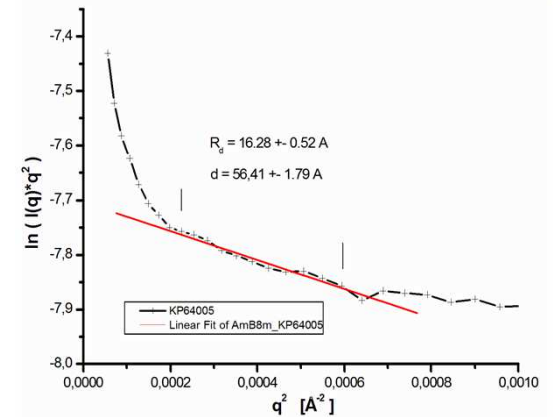


AmB-entrapping core shell nanoparticles : estimation of the shell span by a Kratky-Porod plot evaluation of SANS yields a span radius $R_d = 1.63 \pm 0.052$ nm; i.e a shell span of $d = 5.64 \pm 0.18$ nm, similar to biomembranes (lecithin bilayers ~ 5 nm).

a) R.Johnson, P.Khoshakhlagh, T. Nawroth, P. Langguth, N. Szekely (2014) Eur J Lipid Sci Techn. 116, 1167-73

b) Improvement : AmB in Cholesterol-DOPC (manuscript)

Kratky-Porod plot of SANS of HST particles with Amphotericin B core and Gelatin shell



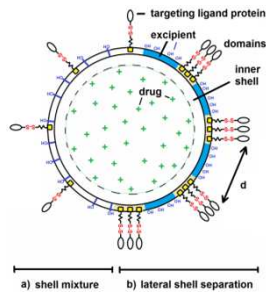
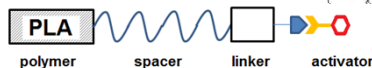
2) Polymer nanoparticles coating by SH-protein + polymer => stable cell targeting nanoparticles

ILL D11

NP with bound protein

150 nm

all in NP-
matching
D₂O
buffer



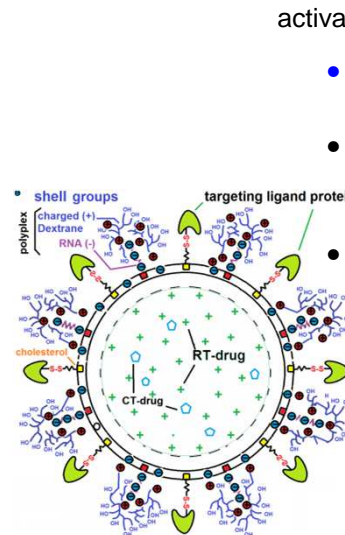
PLGA target nanoparticles
with mixed coatings

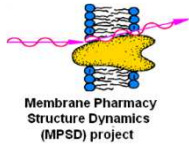
Cooperation: Ralf Schweins ILL Grenoble, LSS group

ILL-D11: TR-SANS + DLS of PLGA NP with activated targeting polymer + protein + lipid-coat

- **D-contrast variation SANS TR-SANS + DLS**
- **D-contrast matched** polymer nanoparticles (PLGA w/o/w) with protein targeting load
- current work: improvements for stabilization by surface coatings
 - **Lipid based** coats, domains
 - **Cholesterol**-stealth coat
 - **C-C-chain** polymer coat (PVA)
 - **Charge coupled** ionic coating (polyplexes with dextrans, mRNA / DEAE-Dextrane)
 - **Hydrophobic drugs** in NP

Twin coating of
D-contrast matched
Polymer nanoparticles
with protein targeting





NEUTRONS
FOR SCIENCE
AND HEALTH

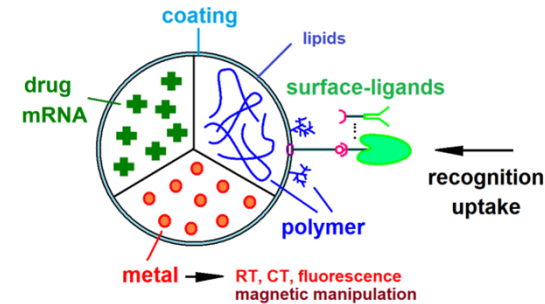


FRM II
Forschungs-Neutronenquelle
Heinz Maier-Leibnitz

HZB
BESSY



Conclusion



jcu UNIVERSITÄT **medizin.**
MAINZ

JOHANNES
GUTENBERG
UNIVERSITÄT
MAINZ

Pharma-
Technology
AK Langguth

- Bio-Medical and Pharmaceutical Nanoparticles are **multicomponent systems** consisting of therapeutic drugs (10%), polymers, lipids, metal oxides (filler) and proteins, which can be distinguished by **neutron scattering with D-contrast variation**
- The **wide size scale** varies from 1 nm (drugs), over ~5 nm (proteins) to the upper 100 nm scale, in several cases up to 200µm. This requires a combination of complementary methods: **SANS + DLS (projecting dual optics, long focal length)**
- The **SANS + DLS combination** can be applied **online** (dual beam) or **offline** (DLS immediately after SANS)
- Metal drug domains can be distinguished by **ASAXS** at the **L-edge**, eg. Erbium+Gd for **cancer radiotherapy**.
- For systems developing in **structure in a process**, e.g. digestion, binding, uptake, SANS and DLS have to be applied as **time resolved methods : TR-SANS + TR-DLS**

SANS Deuterium-contrast variation

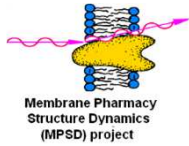
ASAXS energy contrast variation

**SANS
+ DLS / FCPS**

**SANS / SAXS
&
DLS (online)
DLS (offline)**

**TR-SANS / -SAXS
+ TR-DLS**

Thanks



HZB
BESSY

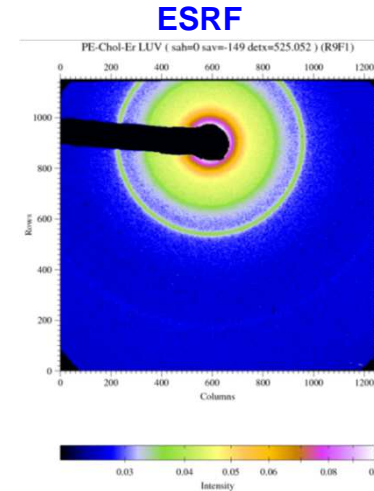
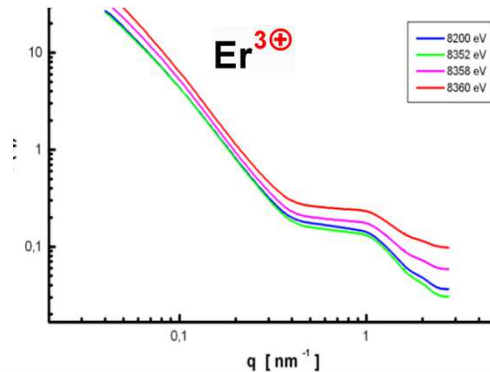
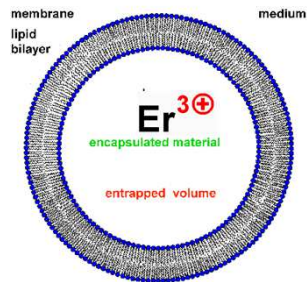
Beam-Target Nanoparticles for Cancer Radio-Therapy

Liposomes and PLGA NP for Radiotherapy by Photons and Neutrons

JOHANNES
GÜTENBERG
UNIVERSITÄT
MAINZ

Pharma-
Technology

Liposome nanoparticles with entrapped Erbium



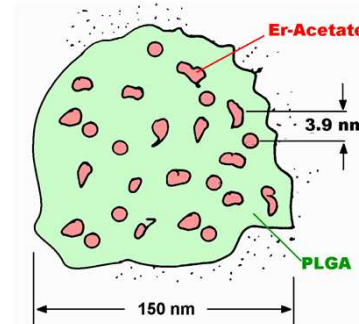
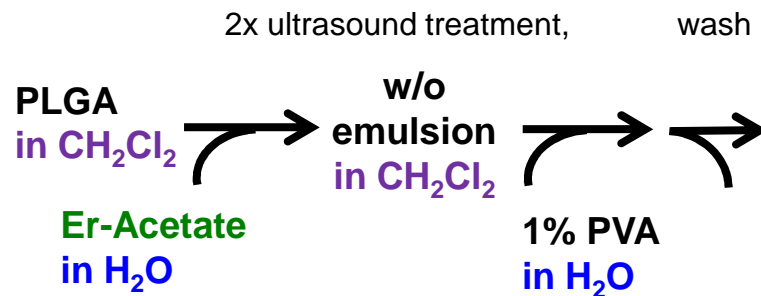
Cooperation:
Peter Boesecke
ESRF
ID01

Cooperation:
Guenther Goerigk
HZB / BESSY
M. Ballauf group

- **Liposomes** from lecithin (DOPC) with entrapped **metal salt** solution (0.5 M)
- **L-edge contrast variation SAXS = ASAXS (5 energies)**
- **Bio-targeting** by protein ligand surface modification

ASAXS & SAXS + DLS (offline) : done at BESSY, option for DESY – PETRA III , P12

PLGA w/o/w nanoparticles (foam-like) with Erbium in domains



ASAXS
@
HZB
BESSY

- **PLGA NP's 10% metal** prepared as w/o/w double emulsion from polymer (PLGA) and metal-salt solution (Erbium-Acetate)
- **L-edge contrast variation SAXS = ASAXS (5 energies)**

JGU Mainz / inventors: Buch K, Nawroth T, Langguth P, Schmidberger H:
European Patent WO 2013/037487 / EP 2 567 702 A1
(2013/12) „Diminishing Cell Growth with Metal-Polymer Nanoparticles upon Radiotherapy“ ... **Metal-PLGA** as example

BMBF project 05KS7UMA

w/o/w double emulsion NP
8 - 10% metal , in H₂O

SANS : @ ILL-D11, Ralf Schweins

Cooperation:
Guenther Goerigk
HZB / BESSY
M. Ballauf group